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# Validation of Online Intrinsic and Reflexive Joint Impedance Estimates using Correlation with EMG Measurements

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# Background

Two <u>state-of-the-art</u> research lines towards <u>voluntary modulation</u> of <u>reflexive activity</u> in order to <u>reduce spasticity</u>:

EMG-based<sup>1</sup>:

- System Identification-based<sup>2</sup>:
- Reduce muscle hyperreflexiaConstant background activity
- Constant intrinsic impedance

Modulation reflexive impedance

- Participants with spasticity
- Able-bodied participants

Can the system identification-based paradigm also be used by participants with spasticity? Potential improvements w.r.t. EMG:

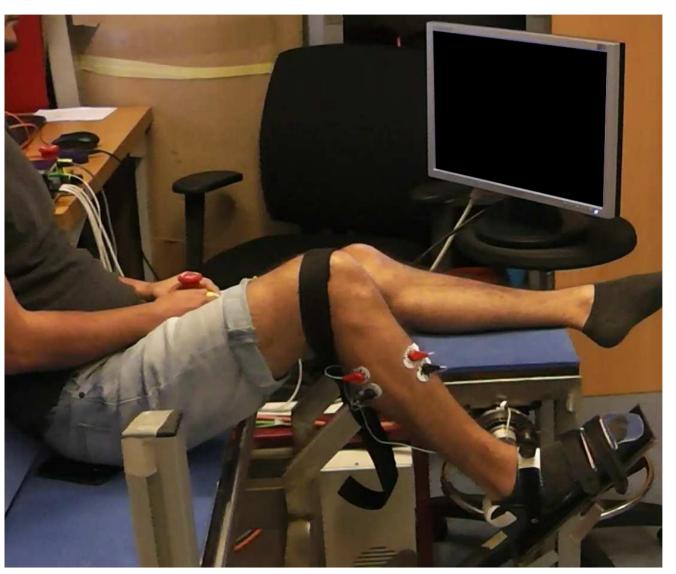
- Participant comfort
- Target multiple muscles
- Applicability
- Faster training effects

#### Aim

Investigate <u>linear association</u> between the <u>independently</u> measured <u>EMG</u>- and <u>system identification</u>-based paradigms:

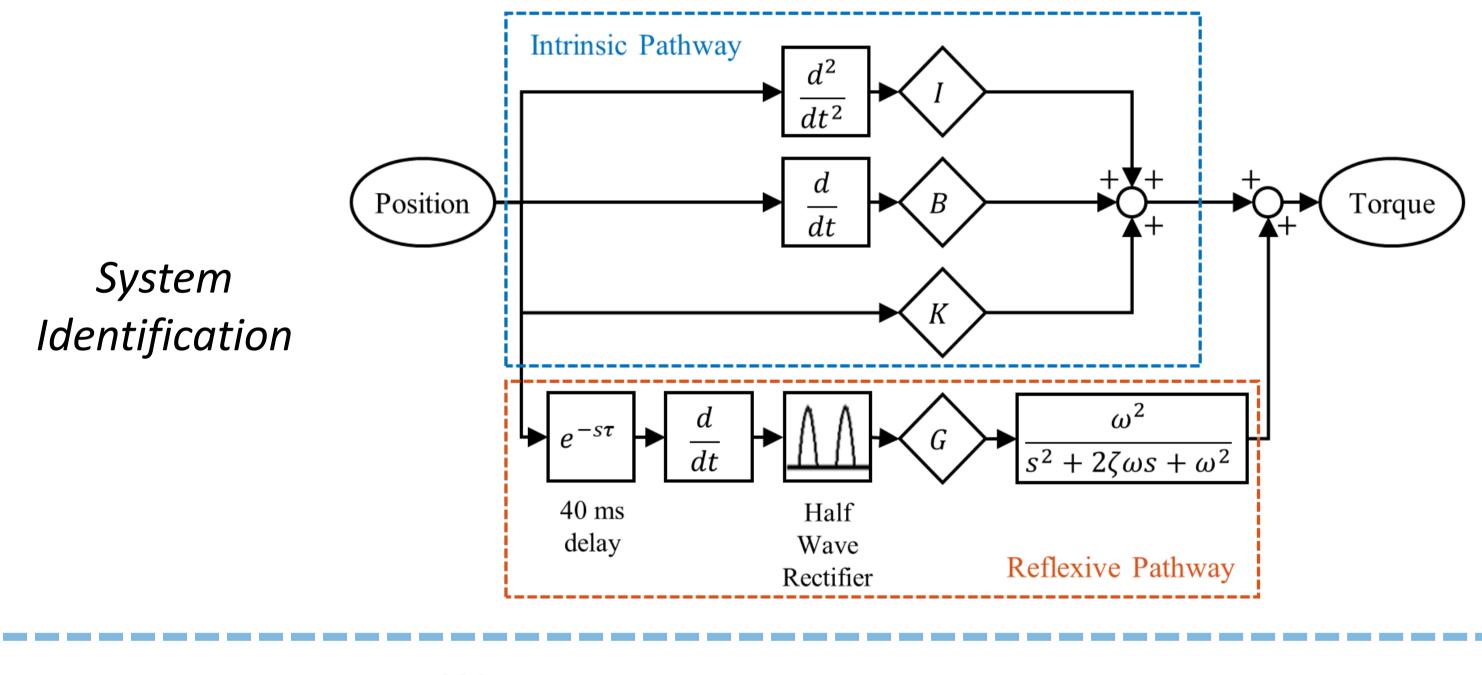
- Background EMG activity ⇔ Intrinsic joint stiffness
- Reflex EMG activity
- ⇔ Reflexive activity

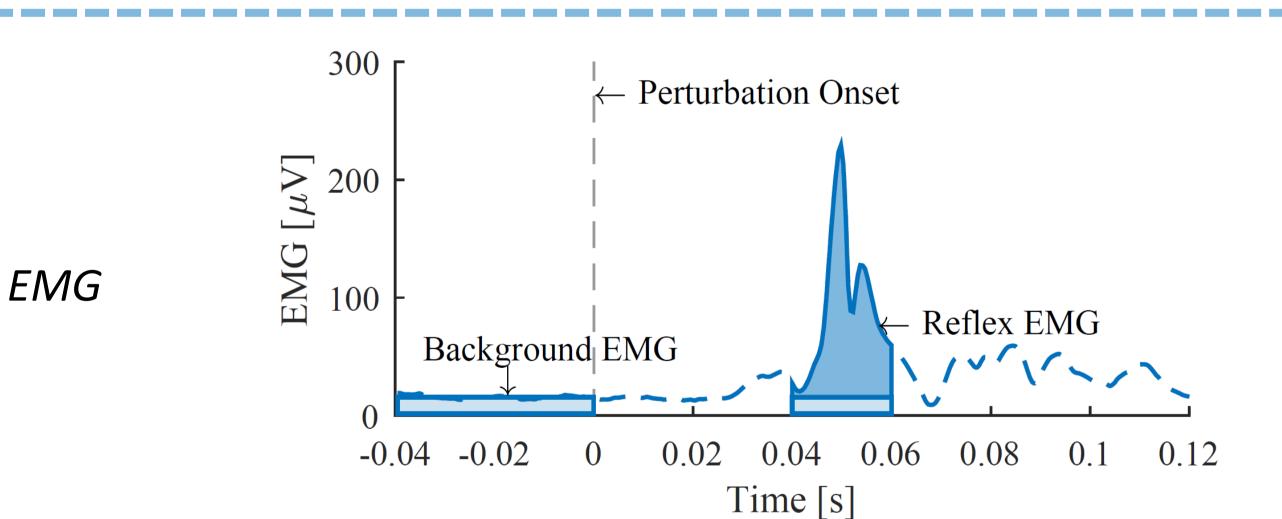
### Protocol



- Today of the second of the sec
- 3 male able-bodied subjects
- 1-DOF perturbations in sagittal plane of ankle joint
- Train modulation intrinsic stiffness & reflexive activity
- Keep behavior constant for several 60s periods
- Feedback on torque (y-axis)
   and intrinsic stiffness or
   reflexive activity (x-axis)
- Neutral or plantarflexion torque task
- Co-contraction allowed

# Methods & Results



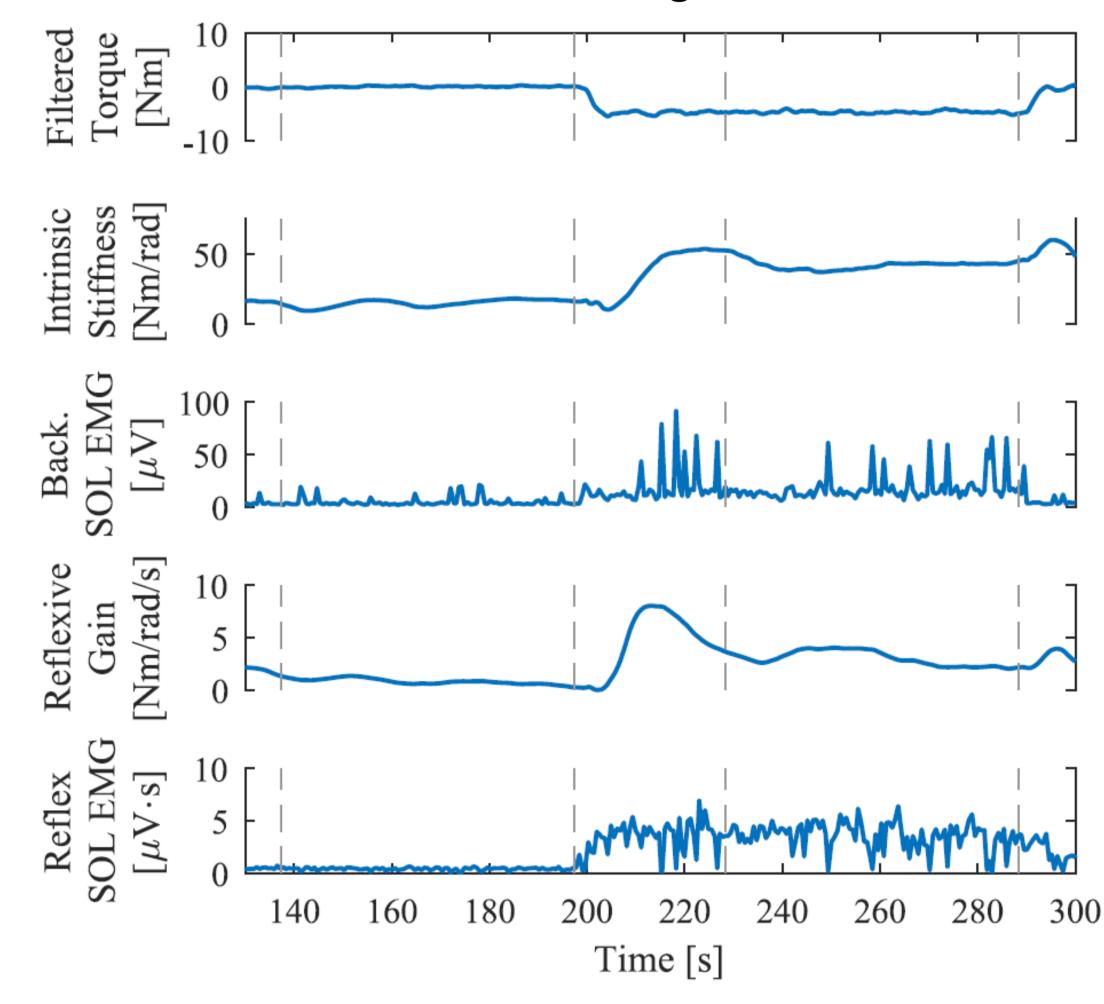


Normalization per subject

# Sub. A Sub. B Sub. C S

# Consecutive 60s periods with constant subject behavior show the following associations:

- Background EMG Soleus ⇔ Intrinsic stiffness



#### Correlation coefficient using data normalized per subject:

	Intrinsic		Reflexive	
Torque	0  Nm  (N = 33)	-5  Nm (N = 22)	0  Nm  (N = 33)	-5  Nm  (N = 22)
SOL	0.93 [0.85, 0.97]	0.70 [ 0.44, 0.87]	$0.78 \ [0.62, 0.87]$	0.57 [ 0.20, 0.77]
TA	0.88  [0.78, 0.95]	0.70 [0.19, 0.87]	0.55 [0.27, 0.75]	0.18 [-0.11, 0.45]
$\operatorname{GL}$	$0.91 \ [0.83, 0.96]$	$0.36 \left[ -0.18, 0.69 \right]$	$[0.75 \ [0.58, 0.85]]$	0.56 [0.21, 0.76]
GM	0.80 [0.56, 0.92]	0.65 [0.32, 0.82]	0.82 [0.67, 0.90]	0.46 [0.13, 0.67]

95% confidence intervals computed for four lower leg muscles and two torque target, via non-parametric bootstrap, show:

- Up to <u>86% shared variance</u> for <u>intrinsic pathway</u>
- Up to 67% shared variance for reflexive pathway

### Conclusions

Valid to use system identification-based approach in training paradigm to reduce muscle hyperreflexia give the large linear association between independent system identification and EMG measures.

# <sup>1</sup> A. K. Thompson, F. R. Pomerantz, and J. R. Wolpaw, "Operant Conditioning of a Spinal Reflex Can Improve Locomotion after Spinal Cord Injury in Humans," *Journal of Neuroscience*, vol. 33, no. 6, pp. 2365–2375, 2013.

# **Future Research**

Recommendations for using system identification measures in training to reduce muscle hyperreflexia:

- Neutral torque task
- Focus on calf muscles

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# UNIVERSITY OF TWENTE.

<sup>&</sup>lt;sup>2</sup>D. Ludvig and R. E. Kearney, "Real-time Estimation of Intrinsic and Reflex Stiffness," *IEEE Transactions on Biomedical Engineering*, vol. 54, no. 10, pp. 1875–1884, 2007.